

THE MATHEMATICAL MODELING OF BRAIN

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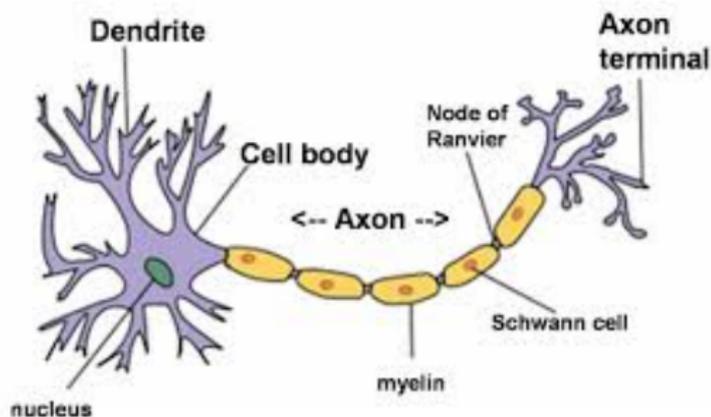
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OUTLINE OF THE TALK

- 1 Introduction
- 2 Evolution of Mathematical Models
- 3 Mathematical Tools
- 4 Applications
- 5 Conclusion

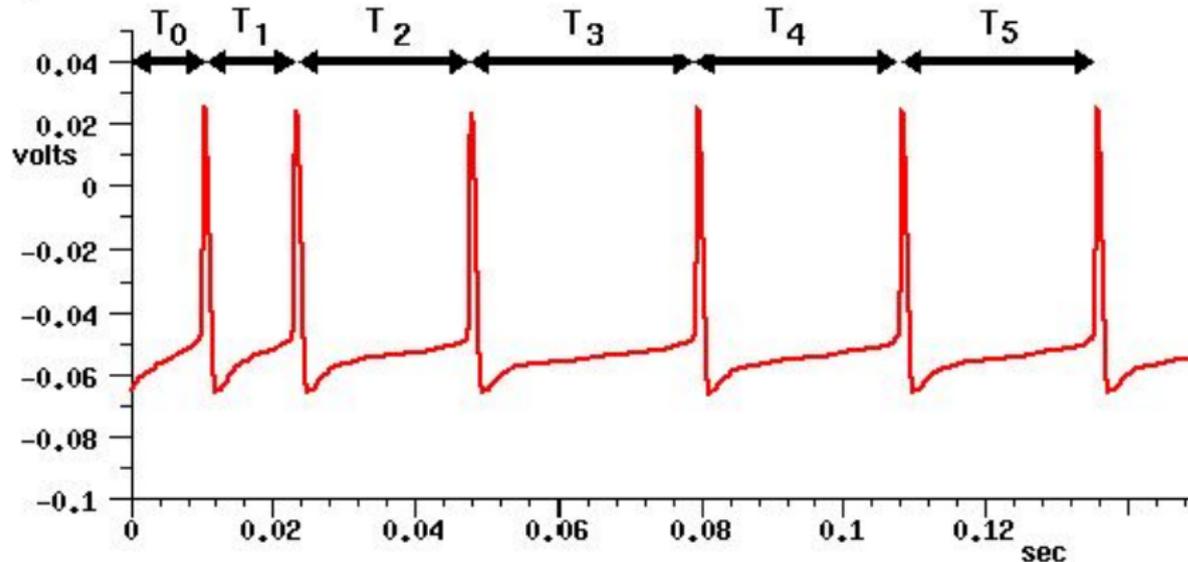
1. INTRODUCTION -THE HUMAN BRAIN

According to a lower estimate from 2009, the human nervous system contains 0.89×10^{11} neurons, which are connected by about 10^{15} synapses.



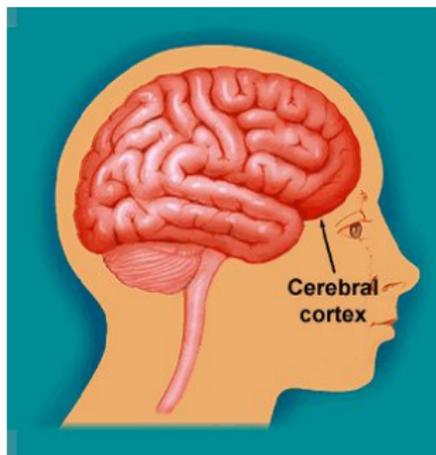
1. COMMUNICATION BETWEEN NEURONS

The **change of voltage** in the cell membrane of a neuron results in a voltage spike called an **action potential**, which triggers the release of other neurotransmitters. That is, **neurons communicate with each other by firing**.



1. THE CEREBRAL CORTEX

The **cerebral cortex** is the brain's outer layer of neural tissue in humans and other mammals. It plays a key role in controlling **memory, attention, perception, awareness, thought, language** and other important processes.



The cortex of a human is about **2-4 mm thick** and contains about **one fifth** of all the neurons. According to recent estimates, the cortex can store up to **100 Tb (10¹⁴ bytes)** of data!

1.DISCOVERY OF NEURON

In the middle of XIX century there were two theories about the structure of nervous cells:

- **Reticularism:** The nervous system consists of a large network of tissue (reticulum);
- **Neuronism:** The nervous systems consists of distinct cells (neurons).

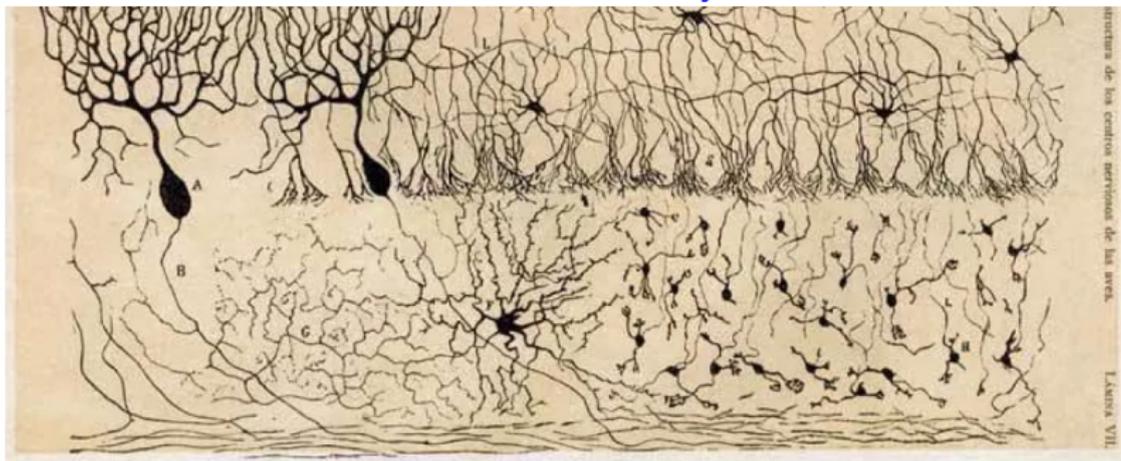


The second theory was defended by **Ramon y Cajal (1852-1938)** who was awarded the **Nobel Prize in Physiology in 1906** (together with Colgi).

1.DISCOVERY OF NEURON

The term **neuron** was introduced in 1891. Ramon y Cajal developed the so-called **Neuron Doctrine**:

- The **neuron** is the structural and functional unit of the nervous system;
- Each neuron is a **distinct cell** which is not fused with others;
- The neuron is composed by **three parts**: dendrites, axon and cell body;
- Information flow : **dendrites** → **cell body** → **axon**.

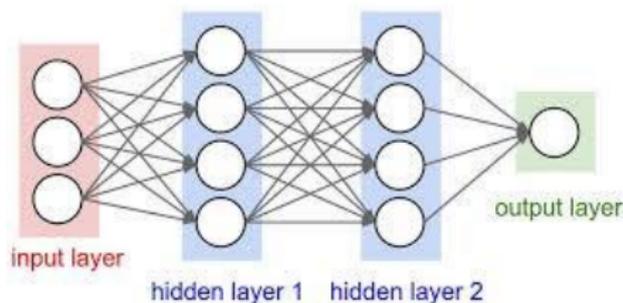


Drawing of the chicken cerebellum by S. Ramon y Cajal

2. NEURAL NETWORKS

The investigation of biological neuron networks in animal brains has inspired the mathematicians to create **artificial neural networks (ANN)**. In 1943 **Warren McCulloch and Walter Pitts** created a computational model for neural networks based on mathematics and algorithms. The original goal of the neural network approach was to solve problems **in the same way that a human brain would**. The **ANN** learns to do tasks by considering examples, generally without task-specific programming. An **ANN** is based on a set of connected units called **artificial neurons**. Each connection (**synapse**) between neurons can **transmit a signal** to another neuron. The receiving neuron can process the signal and then send a new signal to neurons connected to it.

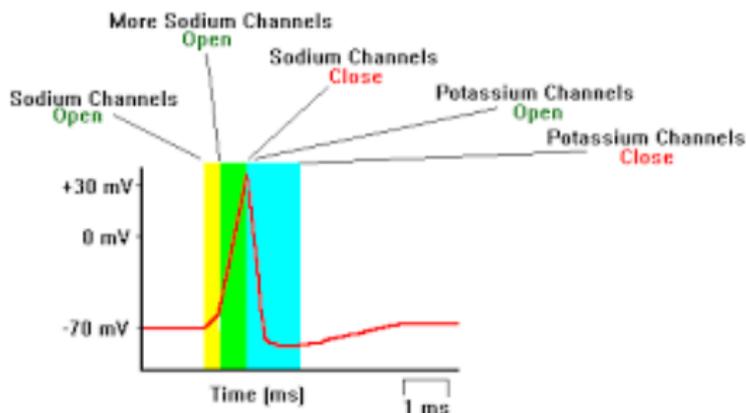
2. NEURAL NETWORKS



Neurons are organized in **layers**. Different layers may perform different kinds of transformations on their inputs. **Signals travel from the first (input), to the last (output) layer.**

Neural networks have been used on a variety of tasks, including computer vision, speech recognition, machine translation, social network filtering.

2. How is an action potential generated?



- The neuron membrane has a certain **resting potential** (about -70mV).
- As a result of **external stimulus**, the membrane potential increases.
- When the membrane potential attains a **certain threshold**, the **sodium channels open**.
- As **sodium ions** flow into the neuron, the membrane potential increases (**depolarization process**).
- When the membrane potential attains a **certain critical value**, the **sodium channels close** and the **potassium channels open**.
- As **potassium ions** flow out of the neuron, the membrane potential decreases (**repolarization process**).

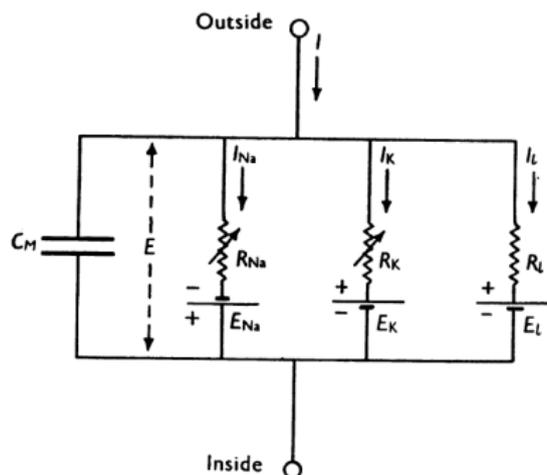
2. How can this process be described by a mathematical model?

In 1952 [A.H. Hodgkin and A.F. Huxley](#) introduced a mathematical model that describes the [ionic mechanism](#) underlying the initiation and propagation of action potentials (nervous stimulus) in an axon.

The Hodgkin-Huxley model describes the ionic exchanges between the [extracellular and intracellular medium](#), using the language of [electric circuits](#) (conductance, capacitance, current sources).

In 1963 [A.H. Hodgkin and A.F. Huxley](#) were awarded the [Nobel Prize in Physiology or Medicine](#) for this work.

2. HODGKIN-HUXLEY EQUATIONS



Hodgkin and Huxley have described **ion currents** in the language of **electric circuits**.

The **ion channels** (sodium, potassium, leaky) are replaced by **electrical resistances** (R_{Na} , R_K , R_L).

The **conductance** in the **leaky channel** is **constant** (the channel is always open). The other channels may **close or open** when the **membrane potential** attains certain critical values.

2. HODGKIN-HUXLEY EQUATIONS

The main physical variables in the description of the ion currents are the **membrane potential** and the **electrical conductances** (sodium, potassium and leaky).

The equation for the membrane potential (V_m):

$$I = C_m \frac{dV_m}{dt} + g_k(V_m - V_k) + g_{Na}(V_m - V_{Na}) + g_l(V_m - V_l)$$

I - current; V_m - membrane potential;

g_k, g_{Na}, g_l - potassium, sodium, and leaky conductances;

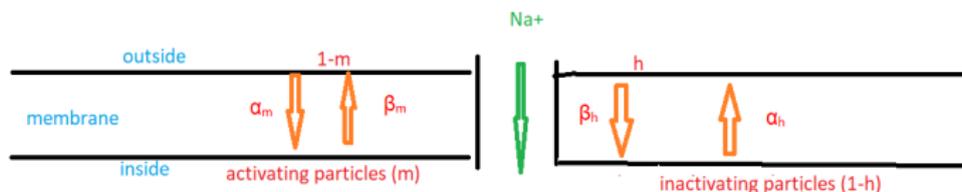
V_k, V_{Na}, V_l - Potassium , sodium, and leaky reversal potentials.

The **leaky conductance** (conductance of the leaky channels) is constant.

The other conductances depend on the membrane potential.

2. How does the sodium conductance change?

There are particles that **activate the sodium channels** and particles that **block** them. These particles can move between inside and outside the membrane.



m - part of the **activation particles** which are inside the membrane.

h - part of the **inactivation particles** which are outside the membrane.

$$g_{Na} = \bar{g}_{Na} m^3 h,$$

\bar{g}_{Na} - maximal value of the sodium conductance.

$\alpha_m, \beta_m, (\alpha_h, \beta_h)$ - **transfer rates** of the activation (inactivation) particles.

Depend on the membrane potential, but not on the time.

2. How does the potassium conductance change?

In the case of potassium, there are only activation particles n - part of the activation particles which are inside the membrane.

$$g_k = \bar{g}_k n^4,$$

\bar{g}_k - maximal value of the potassium conductance.

n satisfies the differential equation:

$$\frac{dn}{dt} = \alpha_n(V_m)(1 - n) - \beta_n(V_m)n.$$

α_n, β_n - transfer rates of the activation particles of the potassium channel.

m and h satisfy similar equations.

2. HODGKIN-HUXLEY EQUATIONS

By coupling the equation for the membrane potential with the equations for n, m, h , we finally obtain a system of **4 nonlinear ordinary differential equations**, known as **Hodgkin-Huxley** equations:

$$I = C_m \frac{dV_m}{dt} + \bar{g}_k n^4 (V_m - V_k) + \bar{g}_{Na} m^3 h (V_m - V_{Na}) + g_l (V_m - V_l)$$

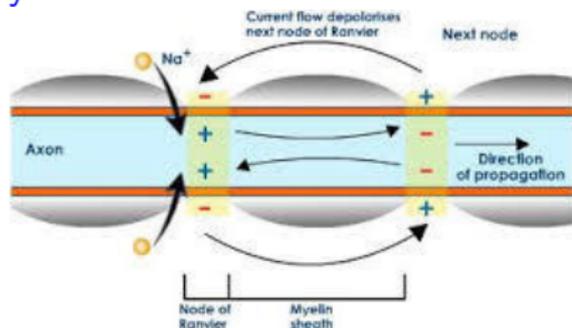
$$\frac{dn}{dt} = \alpha_n(V_m)(1 - n) - \beta_n(V_m)n$$

$$\frac{dm}{dt} = \alpha_m(V_m)(1 - m) - \beta_m(V_m)m$$

$$\frac{dh}{dt} = \alpha_h(V_m)(1 - h) - \beta_h(V_m)h$$

2. FITZHUGH-NAGUMO EQUATIONS

Further investigation of the propagation of nervous stimulus has led to the [FitzHugh-Nagumo equations](#) (1962), which describe the propagation of signals in [myelinated axons](#).

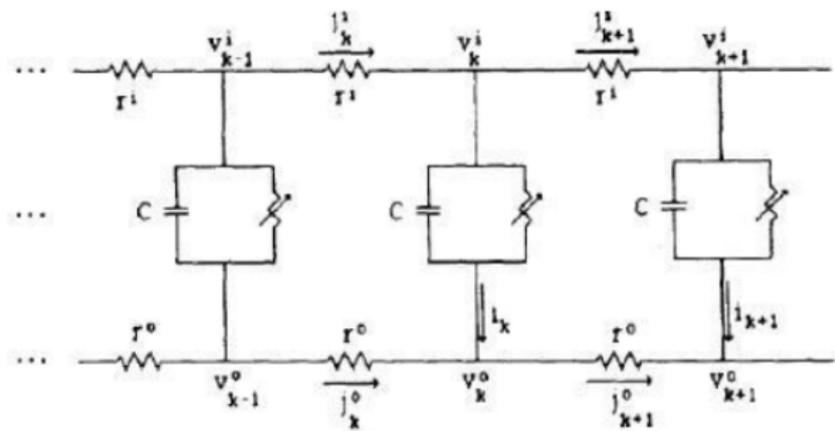


The [myelin](#) completely insulates the membrane, so that all the electric processes occur at the [Ranvier nodes](#).

2. FITZHUGH-NAGUMO EQUATIONS

Circuit Model

Impulse conduction in a myelinated axon can be simulated using a circuit model: the nodes of Ranvier correspond to **condensators** and the space between them, to **resistances**.



2. FITZHUGH-NAGUMO EQUATIONS

Assumptions of the Nerve Conduction Model

- the nodes are **uniformly spaced** and **electrically identical**,
- the axon is **infinite in extent**,
- the cross-sectional variations in potential **are negligible**,
- a supra-threshold stimulus begins a signal which travels down the axon **from node to node**.

2. FITZHUGH-NAGUMO EQUATIONS

The propagation of nervous stimulus can be modeled by the following system of **difference equations**:

$$\begin{cases} \frac{1}{R}(v_{k+1} - 2v_k + v_{k-1}) = C \frac{dv_k}{dt} - f(v_k) + w_k \\ \sigma v_k - \gamma w_k = \frac{dw_k}{dt} \end{cases}, \quad k \in Z, \quad (1)$$

where v_k represents the **membrane potential at the k-th node**, w_k is the so-called **recovery variable**, σ and γ are non-negative rate constants, R and C are the axoplasmic resistance and the nodal membrane capacitance. Equations (1) are known as the **discrete FitzHugh-Nagumo equations**.

2. FITZHUGH-NAGUMO EQUATIONS

The nonlinear function f in [discrete FitzHugh-Nagumo equations](#) represents a current-voltage relation ([activation function](#)) and is supposed to satisfy the following conditions:

$$\begin{aligned} f \in C^1([0, b]), \quad f(0) = f(a) = f(1) = 0, \\ f(v) < 0, \quad \text{if } 0 < v < a; \\ f(v) > 0, \quad \text{if } a < v < 1. \end{aligned} \tag{2}$$

In many applications this function is taken as

$$f(v) = bv(v - a)(1 - v), \tag{3}$$

where $b > 0$.

2. FITZHUGH-NAGUMO EQUATIONS

The discrete FitzHugh-Nagumo equations can be simplified by neglecting the recovery process (that is, it is assumed that the constants σ and γ are so small that **the recovery process has no influence in propagation**). Let us assume that

$$v_{k+1}(t) = v_k(t - \tau),$$

where τ is a certain delay, which is proportional to the space between nodes and to the reciprocal of propagation speed. Then we obtain a **mixed-type functional differential equation**:

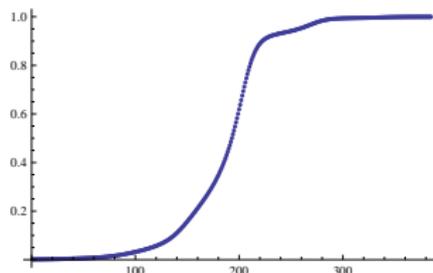
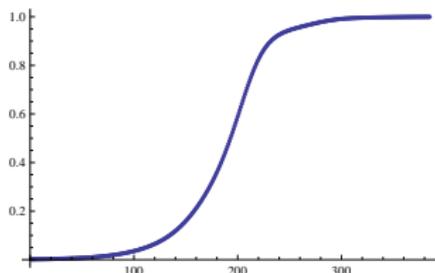
$$\frac{1}{R}(v(t - \tau) - 2v(t) + v(t + \tau)) + f(v(t)) = C \frac{dv(t)}{dt}, \quad (4)$$

2. FITZHUGH-NAGUMO EQUATIONS

Conditions for the existence of solution: $0 < a < 1/2$.

The solution **cannot be solved** by analytical methods.

Numerical solutions a) with $a = 0.1$; b) with $a = 0.3$.



2. POPULATION MODELS

How to describe the activity of a **large population** of N connected neurons ($N \rightarrow \infty$)?

Assumptions (See Gerstner and Kistler, 2001):

- The total number of neurons N remains **constant**.
- The state of neuron i depends explicitly **only on the most recent firing time (t_i) and on the input from other neurons** (but not on firing times of earlier spikes).
- The number of spikes that a network emits on a short time window is the sum of N independent random variables, and therefore converges to its **expectation value**. Hence in a large network we consider expectation values

2. NEURAL FIELDS

A **new approach** to the modeling of neuron populations was introduced in the years 70:

Wilson and Cowan, 1972 and **Amari, 77**

Consider a region Ω of the n -dimensional space and a function $V(\bar{x}, t)$, with $\bar{x} \in \Omega$;

$V(\bar{x}, t)$ represents the spatiotemporal structure of the neuronal population:

- spatial distribution of potential;
- time evolution;

2. NEURAL FIELDS

Neural Field Equation (NFE):

$$c \frac{\partial}{\partial t} V(\bar{x}, t) = I(\bar{x}, t) - V(\bar{x}, t) + \int_{\Omega} K(\|\bar{x} - \bar{y}\|_2) S(V(\bar{y}, t)) d\bar{y}, \quad (5)$$

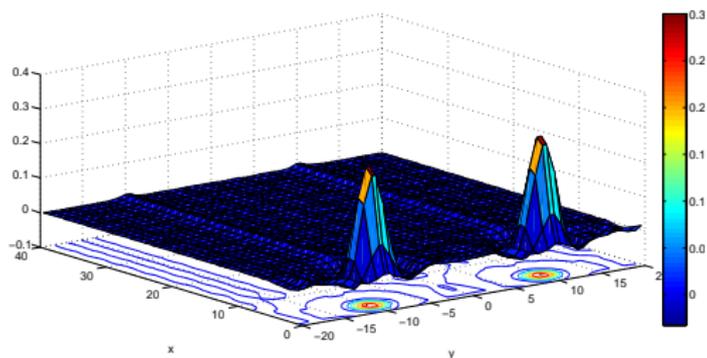
$$t \in [0, T], \bar{x} \in \Omega \subset \mathbb{R}^2;$$

Initial Condition: $V(\bar{x}, 0) = V_0(\bar{x}), \quad \bar{x} \in \Omega.$

- $V(\bar{x}, t)$ - the membrane potential in point \bar{x} at time t ;
- $I(\bar{x}, t)$ - external sources of excitation;
- $S(V)$ - dependence between the firing rate of the neurons and their membrane potentials (sigmoidal or Heaviside function);
- $K(\|\bar{x} - \bar{y}\|_2)$ - connectivity between neurons at \bar{x} and \bar{y} .

2. NEURAL FIELDS

Activation Domain : subset of Ω where the potential is higher than the **threshold**. In this domain there is a **strong connection between neurons**. The stationary solutions of NFE often have one or several activation domains (**multibump solutions**).



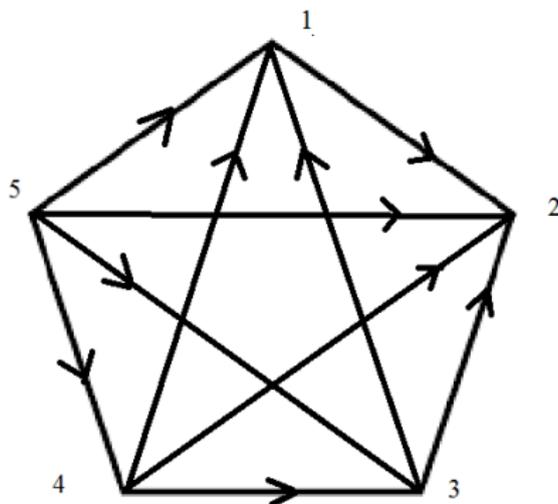
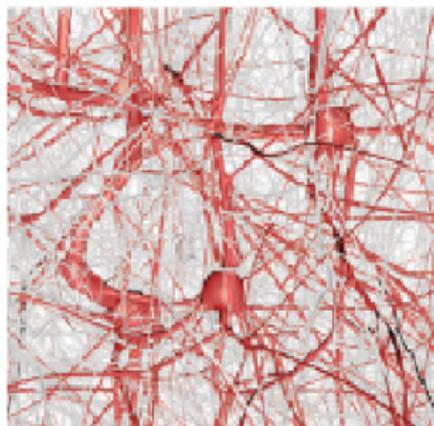
2.ALGEBRAIC TOPOLOGY METHODS

Blue Brain Project

M. Reimann et al., Cliques of Neurons Bound into Cavities Provide a Missing Link between Structure and Function, Frontiers of Mathematical Neuroscience, June 2017.

Construct graphs of a network that **reflect the direction of information flow** and analyse these directed graphs using **algebraic topology**.

2. ALGEBRAIC TOPOLOGY METHODS



clique of neurons	directed graph
neuron	node
synapsis	directed edge
number of connected neurons	dimension

source: node that is source of all edges (5);

sink: node that is target of all edges (2)

2. ALGEBRAIC TOPOLOGY METHODS

directed simplex of dimension $n - 1$ - clique of n all-to-all connected neurons.

Each neuron belongs to many directed simplices of various dimensions. A collection of simplices 'glued' together along common faces forms a simplicial complex.

The space enclosed by directed graphs forming a simplicial complex is called a cavity. The dimension of a cavity is the dimension of the simplices that enclose it.

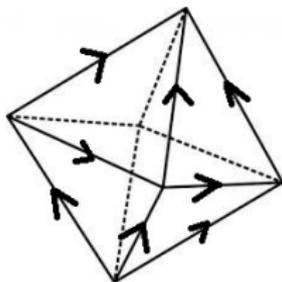
Measures of Topological Complexity of a Simplicial Complex S

Betti number β_n - number of cavities of dimension n enclosed in S .

Euler characteristic - $\chi(S) = \sum_{n \geq 0} (-1)^n |S_n|$, where S_n is the number of n -dimensional simplices contained in S .

2. ALGEBRAIC TOPOLOGY METHODS

EXAMPLE



Betti number - $\beta_2 = 1$ (one 2-dimensional cavity);

$S_0 = 6$ - number of 0-dimensional simplices (vertices);

$S_1 = 12$ - number of 1-dimensional simplices (edges);

$S_2 = 8$ - number of 2-dimensional simplices (faces);

Euler characteristic: $\chi(S) = 6 - 12 + 8 = 2$.

2. ALGEBRAIC TOPOLOGY METHODS

How do the topologic measures of geometrical objects reflect the properties of **neural networks**?

- **Local flow of information** is well described by **directed graphs**;
- **Global measures of information** are given by **Betti numbers** and **Euler characteristic**.

2. ALGEBRAIC TOPOLOGY METHODS

"The variation in Betti numbers and Euler characteristic over time (in response to stimulus) indicates that **neurons become bound into cliques and cavities by correlated activity.**"

"A stimulus may be processed by binding neurons into cliques of increasingly higher dimension, as a specific class of cell assemblies, possibly to represent features of the stimulus."

"The presence of **high-dimensional topological structures** is a general phenomenon across nervous systems".

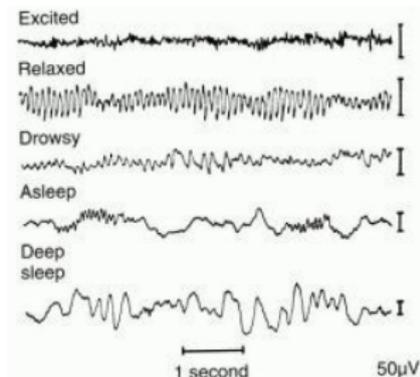
Michael Reinmann et al., 2017

3. MATHEMATICAL TOOLS

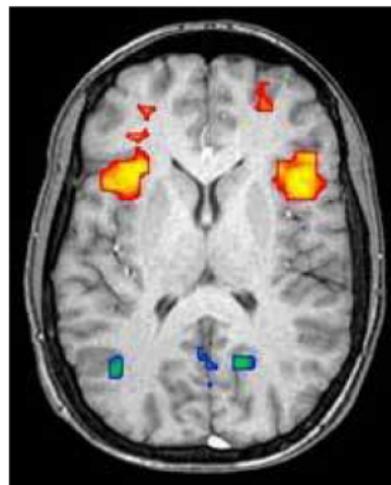
- Differential equations
- Dynamical systems
- Bifurcation theory
- Algebraic topology
- Stochastic processes (essential to take into account the influence of random factors)
- Computational methods (most of the considered equations cannot be solved analytically)

4. APPLICATIONS

INTERPRETATION OF MEDICAL DATA



Output from EEG



Output from fMRI

Neural field models provide a framework for **unifying data** from different imaging modalities, for example, **EEG** (good temporal resolution) and **fMRI** (good spatial resolution).

S. Coombes, 2010

4. APPLICATIONS

NEURAL FIELDS IN ROBOTICS

"To efficiently interact with another agent in solving a mutual task, a robot should be endowed with cognitive skills such as memory, decision making, action understanding and prediction. The proposed architecture is strongly inspired by our current understanding of the processing principles and the neuronal circuitry underlying these functionalities in the primate brain."

W. Erlhagen and E. Bicho, The dynamic neural field approach to cognitive robotics, J. Neural Eng. 3 (2006) R36 – R54

Neural fields are a good tool to simulate working memory.

They simulate how a population of neurons can encode in its firing pattern the features of an external stimulus.

Conclusion

There is a very strong interaction between **Mathematics**, **Neuroscience** and **Informatics**.

- Along the XX century, **Mathematics** has created many powerful tools which gave an important contribution to the investigation of brain and simulation of brain functions.
- **Neuroscience** has contributed to the development of **Mathematics** with experimental data that have given rise to new mathematical models.
- **Mathematics** has also benefited from the development of **Informatics**, which allowed the creation of powerful computers and software tools.
- With all these advances the **simulation of brain functions by artificial devices** became a reality and is developing very fast.

Conclusion

Significant progress obtained in the second decade of XXI century:

- Large amounts of **data**, generated by devices;
- High-performance **computers**;
- Improved **machine learning** algorithms.

This all resulted in **powerfull artificial intelligence systems**.

(Arlindo Oliveira, Former President of IST, expert on artificial intelligence).
It is nowadays possible to replace human by artificial intelligence, but only **for very specific tasks**, which do not require creativity, flexibility of adaptativity. Of course the artificial intelligence will be further developed and improved.

Open question: Will it be possible sometime that artificial intelligence can replace the human brain?

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